

SPECTROSCOPIC PROBE

Field of the Invention

5 This invention relates to a probe for use in spectroscopy, for example Raman or fluorescence spectroscopy. It also relates to a method of manufacturing a component of such a probe.

10 Description of Prior Art

Probes for spectroscopic use are known from, for example, US Patents Nos. 5,112,127 (Carrabba et al) and 5,377,004 (Owen et al).

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The probes shown in those patents are supplied with laser light via an optical fibre, and the laser light is focused by a lens onto a sample. Resulting scattered light, e.g. Raman scattered light or fluorescence at different

20 wavelengths from the laser, is collected by the lens and fed to a second optical fibre, which takes it to a spectroscopic device for analysis. In the Carrabba patent, the scattered light is folded out of the path of the illuminating laser beam within the probe by a beamsplitter.

25 The Owen patent describes an inverse arrangement, in which the scattered light passes in a straight line through the beamsplitter. The beamsplitter acts to fold the illuminating laser light into this beam path, towards the sample.

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In both the Carrabba and Owen patents, the beamsplitter is a dichroic filter. This has several advantages. Firstly, a dichroic filter reflects and transmits the various wavelengths more efficiently than a conventional

beamsplitter. Secondly, it rejects Raman scattering or fluorescence caused by the interaction of the intense laser light with the glass of the optical fibre which delivers the laser light, passing only a monochromatic laser wavelength to the sample. Thirdly, it removes much of the laser wavelength which is back-scattered by the sample along with the desired Raman or other scattered wavelengths. Thus, the desired scattered wavelengths do not become confused in the return optical fibre with Raman scattering or fluorescence induced in the optical fibre by the laser wavelength, which as received from the sample is many times more intense than the desired signals. It also makes it easier to separate the desired wavelengths from the laser wavelength in the spectroscopic apparatus.

In some applications, it would be desirable to miniaturise such a probe. One example is where the probe is to be incorporated in an endoscope for medical examinations, where a maximum diameter of 2mm or less may be desirable. The probes described in the Carrabba and Owen patents comprise numerous discrete components which must be assembled and aligned, making it impossible to achieve such miniaturisation.

25 Summary of the Invention

The present invention, at least in preferred embodiments, seeks to provide a probe having fewer discrete components.

30 One aspect of the present invention provides a component for a spectroscopic probe, comprising a block of transparent material, having two opposed angled faces arranged for reflection of light from one to the other within the block. Preferably at least one of said angled

Fig 2 is an isometric view of part of a sheet of transparent material for use in a method of manufacturing a

Fig 3 shows a portion cut from the sheet of Fig 2, and Fig 4 shows a component of a spectroscopic probe cut from the portion of Fig 3.

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Figure 1 is a schematic representation of the experimental design. It shows a flow from 'Experimental design' to 'Data analysis' and 'Statistical analysis'. 'Experimental design' includes 'Data collection' and 'Data analysis'. 'Data analysis' includes 'Statistical analysis' and 'Data collection'. 'Statistical analysis' includes 'Data collection' and 'Data analysis'.

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The resulting monochromatic beam 32 is then passed to a sampling port, comprising a GRIN lens 22 which focuses the light on the sample to be analysed. Back-scattered light is collected by the lens 22 and passes back to the dichroic surface 12A. Where the lens 22 is a commercially available GRIN type, which is arranged such that its focal plane coincides with its end surface, the end surface may be cut or polished back. This alters the focal plane so that the light can be focused on the surface of the sample, or on sub-surface features of the sample.

The dichroic surface 12A reflects scattered light of the exciting laser wavelength collected by the lens 22, but transmits the desired Raman or fluorescent scattered light 34 into a GRIN lens 24. The lens 24 couples the scattered light 34 into a second, output optical fibre 33, which takes it to a remote spectroscopic apparatus for analysis.

The faces 12A, 12B are preferably parallel to each other and the face 12A, in particular, is preferably angled at a low angle of incidence to the beams, such as 10°. This gives good performance with polarised light, and efficient separation of the laser wavelength from the desired Raman or fluorescent scattered light. However, other angles such as 45° are possible.

The arrangement of Fig 1 reflects the incoming illuminating light at the filter face 12A, to fold it into the same optical path as the scattered light from the sample to the output fibre 33. Whilst that is the preferred arrangement, an inverse arrangement is also possible. In the inverse arrangement, the illuminating light is delivered via the fibre 33 and lens 24 and passes through the filter face 12A to the sample. The scattered Raman or fluorescent light is

As described above, blocks 10 have been produced by cutting the sheet 38 first along the lines 40, then along the lines 41,42. Of course, it is possible instead to cut first

along the lines 41,42 and then along the lines 40.

Using the above method, we have successfully produced spectroscopic probes with diameters of 2mm and less,
5 suitable for use in an endoscope.

The use of GRIN lenses 20,22,24 is not essential. Conventional lenses (or compound groups of lenses) may be substituted.

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One advantage of the probe described is that it can act confocally. The aperture of the fibre 33 acts in a similar manner to a confocal pinhole, so that only light from one focal plane of the sample is accepted and light from other
15 planes is rejected. This gives depth selectivity.

A further possibility is to bundle a plurality of probes according to Fig 1 together, in a single endoscopic instrument. This may be arranged to produce a two-
20 dimensional image of the sample, which may be confocal. Or each probe may point in a different direction, e.g. in a hemi-spherical arrangement, to give a view over a wider area.

25 The miniature probes described may be used in numerous applications where conventional spectroscopic probes would be too large. In addition to endoscopes for in vivo medical and veterinary examinations, they can for example be used in boroscopes for examinations within working
30 machinery and engines.